

A Correlation Study on Motion Artifact using Photodiode and Three Axis Accelerometer Signals

Muhideen Abbas Hasan^{1,2*}, Fahmi Samsuri¹ and Kok Beng Gan³

¹Department of Electrical and Electronics Engineering, University Malaysia Pahang, 26600, Pahang, Malaysia; muhyabass@gmail.com, fahmi@ump.edu.my

²Department of Electronics, Technical Institute/Dour, Northern Technical University, Foundation of Technical Education, Iraq

³Department of Electrical, Electronic, and Systems Engineering, Faculty of Engineering and Built Environment, University Kebangsaan Malaysia, Bangi, Malaysia; gankokbeng@ukm.edu.my

Abstract

Objectives: The three-axis accelerometer used to reflect the Motion Artifact (MA) implemented in the Adaptive Noise Cancellation (ANC) technique has failed to provide the required MA for accurate processing. This study investigates the validity of using a Covered Photodetector (CPD) for MA detection to unify the sources of generated desired and MA signals to avoid electronic noise differences. **Methods/Statistical Analysis:** The two devices were fastened together and exposed to various kinds of motions. The Amplitude Fluctuations (AFs) responding in the time domain and the Linear Correlation Coefficient (r) were observed. **Findings:** Confirmed the proposed approach validity by pointing a rapprochement in AFs. The calculated r was 0.999 in a steady state while in motion states ranges from 0.998 to 0.794 according to movement changes. **Application/Improvements:** Implementing such concept for Photoplethysmography signal processing within ANC leads to a curate critical medical diagnosis at a lower cost.

Keywords: Covered Photodetector, Motion Artifact Reflector, PPG Signal, Three-Axis Accelerometer

1. Introduction

The Photoplethysmographic sensor is an optoelectronic device used to non-invasively measure the continuous change of blood flow in arterial vessels. It uses a LED light source and photodetector assembled into clip probe to monitor the cardiovascular pulse waves that propagate through the blood vessels. Photoplethysmographic (PPG) signals are used to determine the Heart Rate HR, oxygen saturation, Respiratory Rate (RR) and fetal heart rate^{1,2}. They are obscured during movements as a side effect of induced noise by motion, causing an inaccurate reading and interpretation of the PPG signal^{3,4}.

The ANC is one of the several techniques emerged to provide the valid PPG signal in a non-stationary state that it depends on adaptive filtering. The originally induced noise reference is required for updating the fil-

ter coefficients continuously⁵. Two main approaches have been utilized to provide the reference MA, using extra hardwares such as 3-axis accelerometer^{6,7} and synthetic noise signal extracted from the contaminated PPG signal itself^{8,9}. However, the acquired reference signal from those approaches has failed to match the real reflection for entire induced noise due to the motion action. The drawback of first method is, the accelerometer does not reflect the high correlation between motion artifact and the acceleration data¹⁰. For the second method, it is not easy to produce exact estimate computation under the frequency interference of the desired and occurred noise signals especially during fast movements also, it is computationally extensive^{11,12}.

In study¹³, two photodetectors and one LED were utilized whereas in study¹⁴, two LEDs with different wavelengths of Red and Green lights and one photodetector were used. Both studies adopted the differential measure-

*Author for correspondence

ments between the resulting two signals to remove the noise. The reported results were limited to some kind of movements in both works due to difficulties in providing equal amplitudes for two signals during sudden changes of motion as a precondition for effective differential measurements. Therefore, the need for new approach still exists to save the PPG sensor's potential.

In this work, we investigate a new concept to reflect the real induced noise based on generated photocurrent in dark state by the CPD, in order to avoid the difference in electronic noise occurring when a different type of devices are used for obtaining the important signals. An accelerometer is a classic choice to provide the reference MA that actually reflects the change in piezoresistance during motion⁸. Whereas, the PPG signal is a result of counting the photoresistance change¹⁵. Both devices are subjected to the motion and electromagnetic environmental effects due to their nature as electronic equipment, thus causing different types of electronic noise^{16,17} that lead to new negative impacts. Hence, the only way to provide identical MA is to make the desired and resulted noise signals generated from similar twin sources. To validate this concept, several experiments have been conducted on both tied sensors. The three-axis accelerometer and the covered photodetector were undergone to different kinds of motions in the aim to analyze their response under same conditions. Data were collected for six consecutive seconds in silence and motion states along with X, Y, Z, rotating, rolling, walking, and jogging. The results were analyzed through linear correlations criteria which indicated highly positive in sharing close response in reflecting various motions in addition to total correspondence in silence state.

2. Materials and Methods

2.1 Experimental Setup

A custom hardware and software have been designed and developed using Lab VIEW 2015 and DAQ-NI 9215 (National Instruments Corporation). Data were acquired simultaneously from 3-axes accelerometer (AD335, Analog Devices) and traditional PPG sensor type (Nellcor DS-100A) with covered photo-sense area by an optical baffle to prevent the light effect. The generated dark photocurrent is exploited to represent the induced noise that identically generated within corrupted PPG signal at the

same time. The signals were digitized using four channels DAQ-NI 9215 as shown in Figure 1.

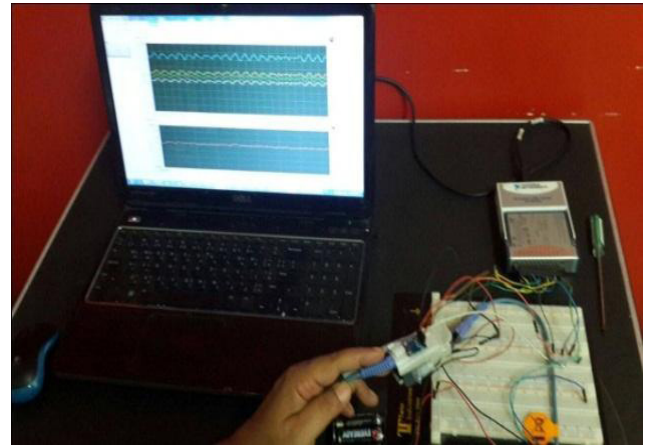


Figure 1. Experimental Setup.

Data was sampled at 100 Hz and 100 samples per channel in six consecutive seconds. In two states of silence without the effect of a fan or air condition just kept on the table trying to achieve the maximum stability. Also seven activities by moving the tied devices along with X, Y, Z axis as well as of rotating, rolling, walking, and jogging. The work has got the Ethical Approval of (IREC 619).

During the computation process for the linear correlation coefficient, the three channel outputs of the accelerometer have been combined using equation (1).

$$Z_x = \sqrt{x^2 + y^2 + z^2} \quad (1)$$

Where Z_x is the combined signal of the 3-axis accelerometer channels X, Y, and Z signals. Whereas, Z_y will represent the resulted signal of the CPD.

2.2 Correlation Study

The goal of a linear correlation analysis is to identify and measure the strength of the relationship between two variables. It is also known as Pearson's correlation coefficient. In all our applications, the combined signal of 3-axis accelerometer will be represented by x whereas the signal of the CPD will be denoted by Y . The equation (2) is used to calculate the linear correlation.

$$r = \frac{\sum Z_x Z_y}{n} \quad (2)$$

where Z_x and Z_y are the standardized Z-values of X and Y . The standardized Z-values indicate how many standard deviations X and Y are above or below the mean.

Moreover, σ and σ^2 are standard deviation and variances respectively and can be determined as in equation (3):

$$\sigma^2 = \sum_{i=0}^{n-1} \frac{(x_i - \mu)^2}{w} \quad (3)$$

where n is the number x elements and μ is the mean of x , which could be calculated as in equation (4).

$$\mu = \sum_{i=0}^{n-1} \frac{x_i}{n} \quad (4)$$

where w is equal to n if weighting is set to population and equal to $(n-1)$ when weighting is configured to sample. The correlation coefficient, r , is always ranging between -1 to 1. When it is one, it means that the two variables are in maximum positive correlation and their data points forms a positive slope line. While the variables x and y are in maximum negative. When r is equal to -1, then the data points gather in the negative slope line. In the case where $r = 0$, it indicates that there is no correlation between both variable, x and y ¹⁸.

3. Results and Discussion

In this section, we discuss the compatibility between the resulting signals of the CPD and accelerometer.

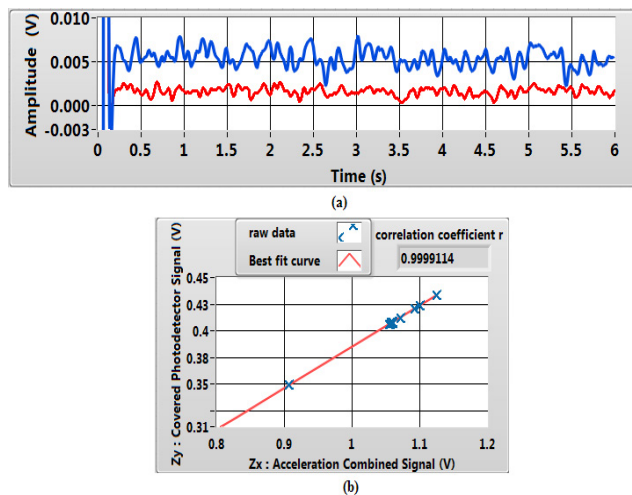


Figure 2. During steady state for continuous six seconds, a) The amplitude fluctuate between the signals of acceleration in Blue and the CPD in Red, (b) Is the linear correlation of acceleration on the X axis and CPD on the Y axis.

3.1 Silence State

this state where there is entirely no motion effect the amplitude fluctuations for the two output signals are

highly convergent, as seen in Figure 2 (a). The linear correlation coefficient (r) is 0.9999, which means the two devices are quite corresponding with each other in reflecting this condition of the steady state as indicated in Figure 2 (b).

3.2 Motion State

In the motion state, amplitude fluctuations for both signals reported lower matching as compared to the matching level in silence state between the two approaches response against the motion, represented by acceleration signal in Blue and CPD in Red as shown in figure 3 (a). The total computed coefficients of linear correlations for the seven activities decreased and ranged from 0.79494 when moving along Y axis to 0.99838 when walking activity was carried out as shown in figure 3(b) and (c), respectively.

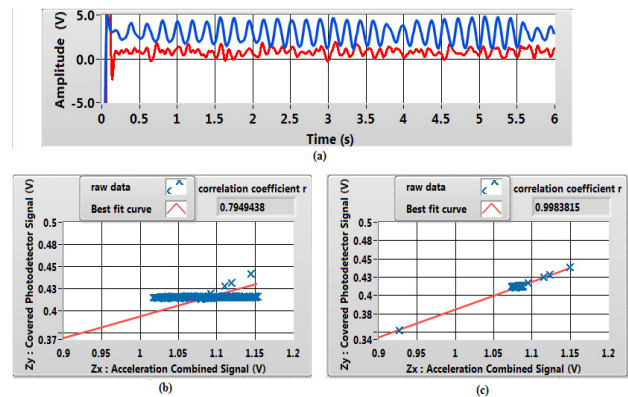


Figure 3. (a) The amplitude fluctuates in motion along the Y axis, (b) and (c) are the maximum and minimum correlation coefficients, between the acceleration and CPD signals, during moving along Y respectively.

Since the two devices are capable of pointing the effect of motion in a convenient extent. More precisely the CPD as a photodetector is designed to convert the light power into electrical energy while the accelerometer is customized to convert the Gravity effect on peso-resistance into electronic signal; they share same ability in sensing and reflecting the motion effect¹⁹. But the critical question is, do the two sensors sense and reflect the same total induced noise (motion artifact) caused by motion in one similar value? The right answer to this inquiry is confirmed by the noticed differences of the resulted linear correlations that the two concepts are not completely matched in indicating the real generated noise.

The minor difference in amplitude trends and linear correlations coefficient as seen in figure 3(a)

and (b) due to electronic noise emergence as a result of different hardware component designs complying with each sensor's function²⁰. Hence, the accelerometer cannot indicate the same noise magnitude that has corrupted the PPG signal which is already generated by a photo detector as would be further explained.

What is notable in Figure 4 is the gradient degradation for the correlation coefficients between the three most significant movements along the X, Z, and Y axis according to their position with the level of the earth surface. The logic interpreter for such case is the accelerometer customized to respond to the phenomena of gravity while the photo detector is a transducer response to light intensity change. The effects of electronic noise in each electronic system is caused by; any degree of free motion, statistical fluctuations of generated current and thermal noise of resistances along with the environmental electromagnetic field^{17,18}.

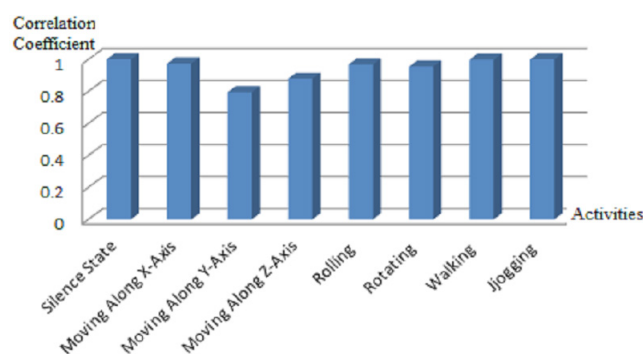


Figure 4. The Various Linear Correlations Coefficients for Reflecting Different Activities within Entire Six Seconds.

The small difference in resulting correlations is very meaningful in the collected measurements of such sensitive and critical PPG signal associated with cardiology diagnosis. Since the covered photo detector is capable of indicating the motions effect through the existed dark photocurrent, it is well qualified to be the best reflector for quite separate MA. The variances occurred in measured r confirm the need for recruiting similar sources to generate the desired and MA signals to meet the most important pre-condition of obtaining the real reference noise for reliable implementation of ANC technique.

4. Conclusion

From the aforementioned outcomes, we can conclude that both concepts have an evenly-matched reaction in vari-

ous states, in the steady state is closest to the absolutely correspondent of 0.99991 in. In motion state, the linear correlations r ranged from 0.79494 to 0.99838 due to the different electronic noise emergence, usually is not taken into consideration during processing such sensitive and informatics signal. These results reinforced the possibility of using covered photo detector as a reliable MA reflector to provide a real reference signal based on generated dark photocurrent in the CPD for precise implementation of ANC in order to process the contaminated PPG signal instead of using the accelerometer. Adopting the new concept opens a new horizon for more specific applications in term of features extraction for various diseases diagnosis with less computational complexities. Practical application of this approach will be presented in our future works.

5. References

1. Jayasree V. Selected cardiovascular studies based on photoplethysmography technique: Citeseer. 2009; p. 1-137.
2. Gan KB, Zahedi E, Ali MAM. Transabdominal fetal heart rate detection using NIR photoplethysmography: instrumentation and clinical results. *IEEE Transactions on Biomedical Engineering*. 2009; 56(8):2075-82. Crossref
3. Rhee S, Yang B-H, Asada HH. Artifact-resistant power-efficient design of finger-ring plethysmographic sensors. *IEEE Transactions on Biomedical Engineering*. 2001; 48(7):795-805. Crossref PMID:11442291
4. Sukor JA, Redmond S J, Lovell N. Signal quality measures for pulse oximetry through waveform morphology analysis. *Physiological measurement*. 2011; 32(3):369-84. Crossref PMID:21330696
5. Zi-Hao Zhang, Jian Liu, Xiao-Yue Wu, Chao-Ying Wang, Ran Yang. A new framework to extract heart rate information from photoplethysmographic (PPG) signals with strong motion artifacts. *TENCON 2015 - 2015 IEEE Region 10 Conference*. 2015; p. 1-4.
6. Gan KB, Zahedi E, Ali MAM. Application of Adaptive Noise Cancellation in Transabdominal Fetal Heart Rate Detection Using Photoplethysmography: INTECH Open Access Publisher. Date accessed: 05/07/201; Available from: <http://www.intechopen.com/books/adaptive-filtering-applications/application-of-adaptive-noise-cancellation-in-transabdominal-fetal-heart-rate-detection-using-photop>.
7. Ram MR, Madhav KV, Krishna EH, Komalla NR, Reddy KA. A novel approach for motion artifact reduction in PPG signals based on AS-LMS adaptive filter. *IEEE Transactions on Instrumentation and Measurement*. 2012; 61(5):1445-57. Crossref

8. Sang Hyun Kim, Dong Wan Ryoo, Changseok Bae. Adaptive noise cancellation using accelerometers for the PPG signal from forehead. 29th Annual International Conference of the IEEE Engineering in Medicine and Biology Society. 2007; p. 2564-7.
9. Asada H H, Hong-Hui Jiang, Gibbs P. Active noise cancellation using MEMS accelerometers for motion-tolerant wearable bio-sensors. The 26th Annual International Conference of the IEEE Engineering in Medicine and Biology Society. 2004; 3:2157- 60. Crossref PMID:17272151
10. Yousefi R, Nourani M, Ostadabbas S, Panahi I. A motion-tolerant adaptive algorithm for wearable photoplethysmographic biosensors. IEEE Journal of Biomedical and Health Informatics. 2014; 18(2):670-681. Crossref PMID:24608066
11. Zhou C, Feng J, Hu J, Ye X. Study of Artifact-Resistive Technology Based on a Novel Dual Photoplethysmography Method for Wearable Pulse Rate Monitors. Journal of Medical Systems. 2016; 40(3):1-10. Crossref PMID:26645320
12. Motion artifact cancellation for wearable photoplethysmographic sensor: Massachusetts Institute of Technology. Date Accessed: 2010; Available from: Crossref
13. Temko A. Estimation of heart rate from photoplethysmography during physical exercise using Wiener filtering and the phase vocoder. 2015 37th Annual International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC). 2015; p. 1500-3.
14. Operation Devices. Date Accessed: 2016; Available from: <http://www.cambridge.org/catalogue/catalogue.asp?isbn=9780521875103>.
15. Mems accelerometers. University of Ljubljana Faculty for mathematics and physics. Date Accessed: 2016; Available from: <http://www.camarabrasilchina.com.br/blog/dopewabere>.
16. Photonic Devices. Date Assessed: 2016; Available from: <http://www.cambridge.org/catalogue/catalogue.asp?isbn=0511074018>.
17. Gabrielson B. Fundamental noise limits for miniature acoustic and vibration sensors. Journal of Vibration and Acoustics. 1995; 117(4):405-10. Crossref
18. Radeka V. Low-noise techniques in detectors. Annual Review of Nuclear and Particle Science. 1988; 38(1):217-77. Crossref, Crossref
19. Stockburger D. Introduction to Statistics: Concepts, Models and Applications. Date Accessed: 1996; Available from: <https://www.fmi.uni-sofia.bg/fmi/statist/education/IntroBook/sbk00.htm>.
20. Webster JG, Eren H. Measurement, Instrumentation, and Sensors Handbook: CRC Press: Spatial, Mechanical, Thermal, and Radiation Measurement. 2 nd (edn). 2014; p. 1640.